

# Optical Coherence Tomography

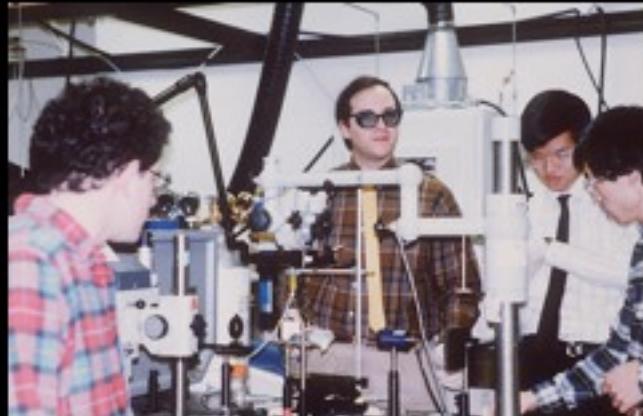
**JOEL S. SCHUMAN, MD**

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PROFESSOR, CENTER FOR THE NEURAL BASIS OF COGNITION  
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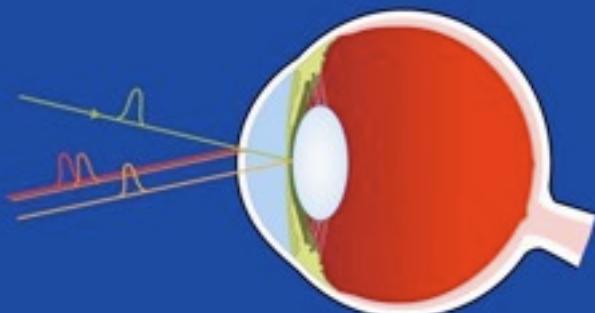
## Disclosures

As an inventor of Optical Coherence Tomography (OCT), Dr. Schuman receives royalties for intellectual property owned by MIT and licensed to Carl Zeiss Meditec, Inc.

## OCT Development



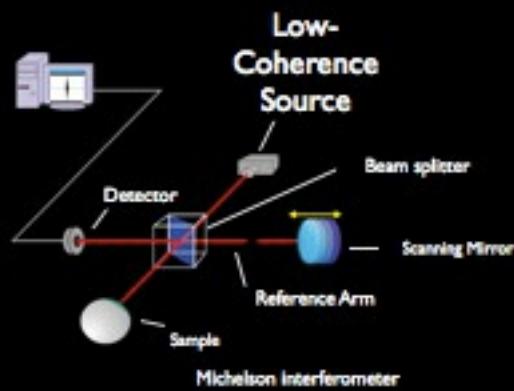
## OCT is Based on Optical Ranging



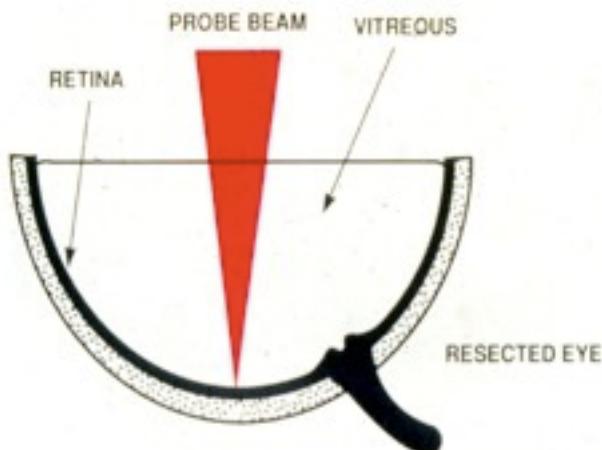
Depth = 0.5 Time-of-Flight / Speed-of-Light

## OCT Principle

A superluminescent diode serves as the light source for an interferometer-based fiber-optic system. The light beam is scanned transversely across the eye, analogous to B-mode ultrasound, to produce a cross-sectional image of the tissue of interest. In this case the retina and optic nerve head (ONH)

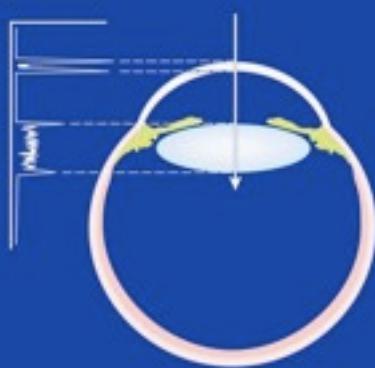


## RETINAL MEASUREMENT SETUP

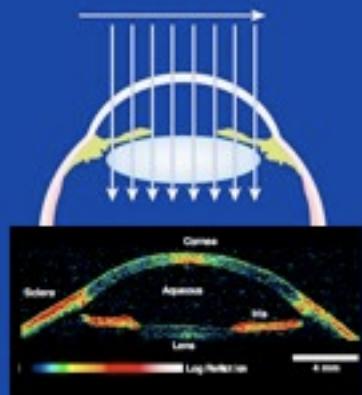


# OCT Scanning

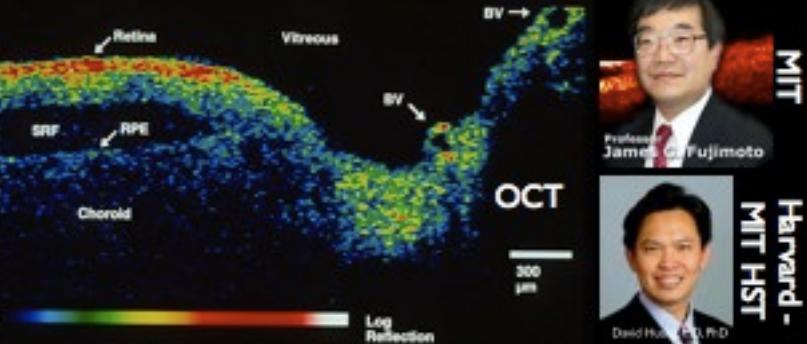
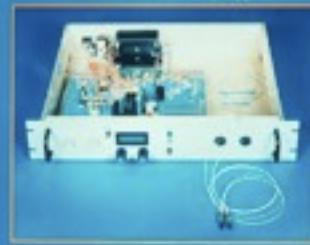
Axial Scan



Transverse Scan



ODDR OPTOELECTRONICS



OCT

300  $\mu$ m

MIT  
Harvard -  
MIT HST

## Optical Coherence Tomography

DAVID HSIAO, ERIC A. SWANSON, CHARLES P. LIN,  
JOEL S. SCHUMAN, WILLIAM G. STINSON, WARREN CHENG,  
MICHAEL R. HEE, THOMAS FLITTE, KENTON GREGORY,  
CARMEN A. PULIAFITTO, JOSHUA G. FUJIMOTO\*

A technique called optical coherence tomography (OCT) has been developed for noninvasive cross-sectional imaging in biological systems. OCT uses low-coherence interference to generate a longitudinal image of tissue by detecting the intensity of those microreflections in a way similar to ultrasonic pulse-echo imaging. OCT has longitudinal and lateral spatial resolutions of a few micrometers and can detect reflected signals as small as  $\sim 10^{-10}$  of the incident optical power. Tomographic imaging is demonstrated *in vivo* in the peripapillary area of the retina and in the coronary artery, two clinically relevant examples that are representative of transparent and turbid media, respectively. *Science* Vol. 284 (No. 5422, 1999), 1179-1181



Histology

## Commercial OCT Systems



# OCT Today

## Spectral-Domain Optical Coherence Tomography: A Comparison of Modern High-Resolution Retinal Imaging Systems

DANIEL F. KIERNAN, WILLIAM F. MILLER, AND MEENAKSHI HARIPRASAD  
*Am J Ophthalmol* 2010;149: 10–31

TABLE. Commercially Available Spectral-Domain Optical Coherence Tomography Systems

System (Company)	Axial Resolution (μm)	# Scans per Second <sup>a</sup>	Advanced Features <sup>b</sup>
Cirrus HD-OCT (Carl Zeiss Meditec)	8	27,000	Fluence-independent scan adjustment; multi-layer en face OCT visualization; high-resolution anterior segment imaging
Spectralis (Heidelberg Engineering)	7	40,000	Point-to-point registration with eye tracking; Up to 4 diagnostic methods in 1 platform; digital resolution to 3.5 μm; improved choroidal visualization
RTVue-100 (Optos)	6	29,000	10 mm long macula scans can be overlapped; Point-to-point registration with eye tracking; choroid analysis and Doppler blood flow characterization; high-resolution anterior segment imaging
SD-OCT 1000 SD-OCT 1000P (Rapport)	6	18,000	Nanoimager camera provides color fundus photographs; Capable of exporting to common multimedia devices; able to import three-domain (spectra OCT) images
Spectralis (OCT-1000) IDPRO-OCT	6	27,000	Point-to-point registration with eye tracking; microperimetric; macular analysis; high-resolution anterior segment imaging
SD-OCT Copernicus (Optos)	6	25,000	Point-to-point registration with eye tracking; high-resolution anterior segment imaging; can separate and view all-retinal layers; software allows inferential cyst volumetric analysis
SD-OCT Copernicus HPR (Carl Zeiss Meditec, Inc.)	5	30,000	High-resolution and fastest speed of available device; multi-layer en face; Doppler retinal blood flow analysis
SD-OCT (Bausch)	6	20,000	Handheld head for procedures or office or ambulatory research; portability facilitates use in an operating room; Doppler retinal blood flow analysis
RetinaScan PRO-2000 <sup>c</sup> (Nidek)	7	55,000	Segmentation analysis of 6 distinct retinal layers

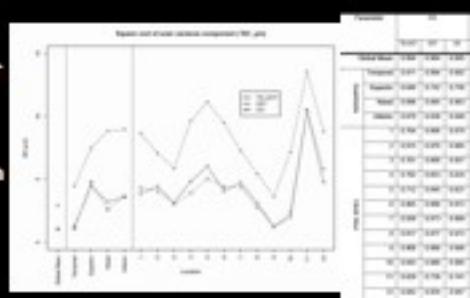
OCT = optical coherence tomography

<sup>a</sup>Based on a review of available data at the time the manuscript was prepared.

<sup>b</sup>Not yet approved by the Food and Drug Administration.

# Reproducibility

- SD-OCT showed statistically significantly better RNFL thickness measurement reproducibility than TD-OCT
- Re-sampling circle location variation on the SD-OCT was relatively small from scan to scan
- No statistically significant difference was detected between Center Each Time and Center Once methods



Kim JS, Ishikawa H, Sung KK, Xu J, Wollstein G, Silcox RA, Gabriele HL, Kragemann L, Duke J, Fujimoto JG, Schwartz JS. Retinal nerve fiber layer thickness measurement reproducibility improved with spectral domain optical coherence tomography. *Br J Ophthalmol*. 2009 Aug;93(8):1057-63. Epub 2009 May 7.

## Reproducibility of RTVue Retinal Nerve Fiber Layer Thickness and Optic Disc Measurements and Agreement with Stratus Optical Coherence Tomography Measurements

ALBERTO O. GONZÁLEZ-GARCÍA, GIANMARCO VIZZERI, CHRISTOPHER BOWD, FELIPE A. MEDEIROS, LINDA M. ZANGWILL, AND ROBERT N. WEINREB

*Am J Ophthalmol* 2009;147:1067-1074

TABLE 2. Reproducibility of RTVue Retinal Nerve Fiber Layer Thickness Measurements in Healthy Participants and Glaucoma Patients

RNFL Parameters	Healthy Participants			Glaucoma Patients				
	Mean (SD) Cr	Sd = 1.04 mm	CV %	ICC (95% Cr)	Mean (SD) Cr	Sd = 1.06 mm	CV %	ICC (95% Cr)
TEMP (μm)	80.8 (7.7) to 83.8	2.87 ± 0.38	3.5%	0.89 (0.88 to 0.90)	77.2 (88.7 to 73.8)	3.38 ± 0.7	4.7%	0.86 (0.81 to 0.91)
SUP (μm)	120.8 (11.7) to 124.3	3.8 ± 0.57	3.1%	0.97 (0.96 to 0.98)	102.2 (98.8 to 106.8)	3.87 ± 0.36	3.3%	0.93 (0.89 to 0.96)
NAS (μm)	75.8 (7.2) to 79.7	2.84 ± 0.44	3.8%	0.97 (0.96 to 0.98)	88.6 (98.2 to 71.3)	3.22 ± 0.52	4.8%	0.89 (0.83 to 0.92)
INF (μm)	134.3 (39.7) to 106.8	8.53 ± 0.95	3.6%	0.95 (0.93 to 0.97)	113.2 (108.9 to 117.4)	3.21 ± 0.46	3.6%	0.96 (0.94 to 0.97)
Avg (μm)	100.8 (9.6) to 105.4	1.57 ± 0.27	1.5%	0.97 (0.95 to 0.99)	99.1 (86.5 to 91.7)	1.66 ± 0.23	1.8%	0.97 (0.96 to 0.98)

AVG = average quadrant; CI = confidence interval; CV = coefficient of variation; ICC = intraclass correlation coefficient; INF = inferior quadrant; NAS = nasal quadrant; SUP = superior quadrant; Sd = within-subject standard deviation; RNFL = retinal nerve fiber layer; TEMP = temporal quadrant.

Reproducibility is expressed as the sde, the ICC, and the CV. Sde is defined as the square root of the within-subject variance (defined as the within-subjects sum of squares divided by its degrees of freedom). CV is calculated as the square root of the residual mean squared values of 3 measures, divided by mean.

## Reproducibility of RTVue Retinal Nerve Fiber Layer Thickness and Optic Disc Measurements and Agreement with Stratus Optical Coherence Tomography Measurements

ALBERTO O. GONZÁLEZ-GARCÍA, GIANMARCO VIZZERI, CHRISTOPHER BOWD, FELIPE A. MEDEIROS, LINDA M. ZANGWILL, AND ROBERT N. WEINREB

*Am J Ophthalmol* 2009;147:1067-1074

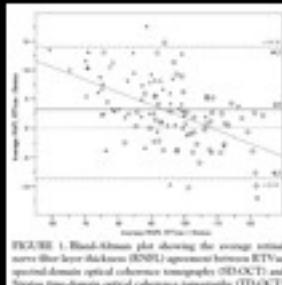


FIGURE 1. Bland-Altman plot showing the average retinal nerve fiber layer thickness (RNFL) agreement between RTVue optical-domain optical coherence tomography (SD-OCT) and Stratus time-domain optical coherence tomography (TD-OCT) in healthy persons (circle) and glaucoma patients (triangle).

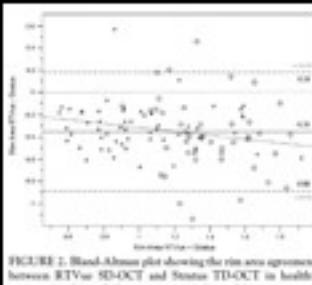


FIGURE 2. Bland-Altman plot showing the rim area agreement between RTVue SD-OCT and Stratus TD-OCT in healthy persons (circle) and glaucoma patients (triangle).

## Comparison of Retinal Nerve Fiber Layer Measurements Using Time Domain and Spectral Domain Optical Coherence Tomography

John J. Wright, MD,<sup>1</sup> Robert T. Chang, MD,<sup>2</sup> Wilson J. Evans, MD,<sup>2</sup> David J. Shattock, MD,<sup>2</sup> Michael J. Hodge, MD,<sup>3</sup> Christopher Warkentin-Lynch, MD,<sup>3</sup> Daniel J. Frazee, MD,<sup>3</sup> Robert M. Williams, MD,<sup>3</sup> Christopher C. Lee, MD,<sup>3</sup> Paul G. Johnson, MD,<sup>3</sup> Deep Patel, MD,<sup>3</sup> and Alan D. Moore, MD,<sup>3</sup> *From the <sup>1</sup>Glaucoma Center, Department of Ophthalmology, University of Michigan, Ann Arbor; <sup>2</sup>Department of Ophthalmology, University of Michigan, Ann Arbor; and <sup>3</sup>Department of Ophthalmology, University of Michigan, Ann Arbor, MI*

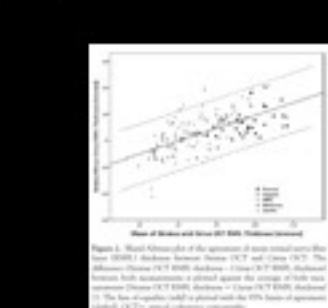


FIGURE 1. Mean RNFL thickness of the apparent RNFL measured with Stratus OCT and Cirrus OCT. The mean of Stratus and Cirrus OCT RNFL thickness measurements was plotted against the average of both measurements. A linear regression analysis was performed using the PIVS linear least-squares method. Stratus OCT = spectral-domain OCT; Cirrus OCT = optical coherence tomography.

**Conclusions:** RNFL thickness measurements between Stratus OCT and Cirrus OCT cannot be directly compared. Clinicians should be aware that measurements are generally higher with Stratus than with Cirrus except when the RNFL is very thin, as in severe glaucoma. This difference must be taken into account if comparing Stratus measurements with Cirrus measurements.

## Diagnostic Ability of Fourier-Domain vs Time-Domain Optical Coherence Tomography for Glaucoma Detection

MITRA SEHLI, DILRAJ S. GREWAL, CLINTON W. SHEETS, AND DAVID S. GREENFIELD

*Am J Ophthalmol 2009;148:917–925*

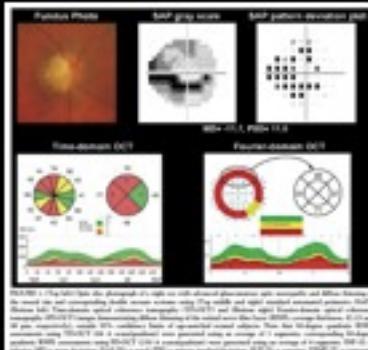


FIGURE 1. FD-OCT has the potential to offer an additional dimension with diagnostic and therapeutic value. However, the clinical validity of FD-OCT remains to be determined. In this study, we compared the diagnostic performance of FD-OCT and TD-OCT in detection of glaucomatous damage. We found that FD-OCT had similar diagnostic performance to TD-OCT in detection of glaucomatous damage. However, FD-OCT was more powerful than TD-OCT in detection of preperimetric glaucomatous damage. FD-OCT = Fourier-domain OCT; SDP = scanning laser polarimetry.

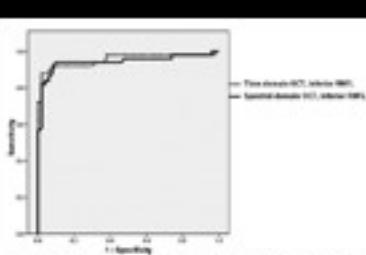


FIGURE 2. Graph showing the area under the receiver operator characteristic curves (AUROCs) for the best parameter obtained using TD-OCT (inferior RNFL thickness; AUROC = 0.95) and FD-OCT (inferior RNFL thickness; AUROC = 0.94;  $P = .45$ ).

## Glaucoma

### Comparison of Cirrus OCT and Stratus OCT on the Ability to Detect Localized Retinal Nerve Fiber Layer Defects in Preperimetric Glaucoma

Jin Wooh Jeoung<sup>1,2</sup> and Ki Ho Park<sup>1,2</sup>

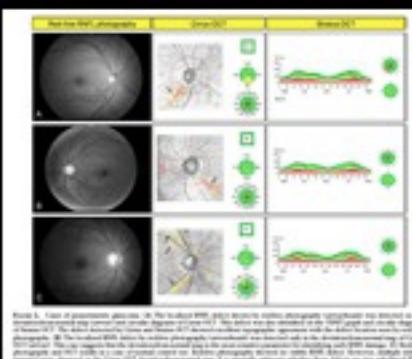


FIGURE 1. Axial RNFL photographs (A) and localized RNFL defects (B) detected with Cirrus OCT and Stratus OCT. The localized RNFL defects were detected only by the Stratus OCT device in the glaucomatous eyes (C, D). Axial RNFL photographs are not visible in a grayscale color map, whereas photographs detected by the Stratus OCT device are clearly visible in the grayscale color map. The localized RNFL defects detected by the Stratus OCT device were not detected by the Cirrus OCT device. Cirrus OCT = Cirrus OCT; Stratus OCT = Stratus OCT.

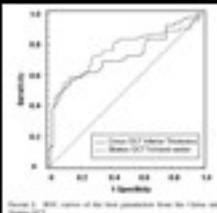


FIGURE 2. ROC curve of the false-positive rate for Cirrus OCT and Stratus OCT. Cirrus OCT = Cirrus OCT; Stratus OCT = Stratus OCT.

**Conclusion:** There were no significant differences between the AUCs for Cirrus and Stratus OCT, indicating that the two devices have similar diagnostic potential in preperimetric glaucoma. After comparison with their nominal databases, Cirrus OCT had greater diagnostic sensitivity; however, Cirrus OCT had a higher cost for lower specificity than Stratus OCT (mean 106,115\$).

# Comparison of Retinal Nerve Fiber Layer Thickness Measured by Cirrus HD and Stratus Optical Coherence Tomography

Kyung Kim Sung, MD, Dong Yoon Kim, MD, Sung Ilse Park, MD, Michael S. Kook, MD  
Ophthalmology 2009;116:1264–1270

Table 1. Clinical Characteristics of the Study Population

	Glasses (n = 147)	OS (n = 147)	Healthy (n = 88)	P Value
Age (mean ± SD)	51.5 ± 10.9	51.5 ± 11.7	51.5 ± 12.8	0.31
SD (range ± SD)	± 10.4 (17.0–65.0)	± 10.4 (17.0–65.0)	± 10.4 (17.0–65.0)	>0.001
Mean RNFL (μm)	112.4 ± 11.7	112.4 ± 11.7	113.0 ± 11.7	>0.001
Average RNFL	112.2 ± 11.7	112.3 ± 11.7	113.0 ± 11.7	>0.001
Thickness by Stratus OCT				>0.001
(mean) (μm)	112.4 ± 11.7	112.4 ± 11.7	113.0 ± 11.7	>0.001
Standard deviation	11.2 ± 11.7	11.2 ± 11.7	11.3 ± 11.7	>0.001
Thickness by Cirrus HD-OCT				>0.001
(mean) (μm)	112.4 ± 11.7	112.4 ± 11.7	113.0 ± 11.7	>0.001
SD (range)	± 10.4 (17.0–65.0)	± 10.4 (17.0–65.0)	± 10.4 (17.0–65.0)	>0.001

ANCOVA = analysis of covariance; OS = glaucoma suspect; SD = mean deviation; OCT = optical coherence tomography; PBD = patient-based deviation; RNFL = retinal nerve fiber layer; SD = standard deviation.  
\*Comparative P value between OS and healthy by post hoc Tukey test.  
†Comparative P value between OS and healthy by post hoc Tukey test.

Table 4. Sensitivity and Specificity (%) of Stratus Optical Coherence Tomography (OCT) and Cirrus HD-OCT

Parameter	OCT	Sensitivity, %		Specificity, %	
		95% CI	95% CI	95% CI	95% CI
Average RNFL	Stratus OCT	40.0 (27.5–54.0)	96.2 (90.5–99.4)		
	Cirrus HD-OCT	43.6 (40.5–75.0)	100.0 (92.5–100.0)		
SD (range)	Stratus OCT	34.4 (27.0–41.7)	97.7 (91.7–99.7)		
	Cirrus HD-OCT	26.8 (14.2–86.7)	96.2 (90.2–99.4)		
SD (range)	Stratus OCT	11.7 (10.6–40.0)	90.2 (78.8–95.0)		
	Cirrus HD-OCT	81.8 (68.6–92.5)	93.3 (72.2–94.4)		

RNFL = retinal nerve fiber layer.

Conclusions: There were significant differences in RNFL thickness and normative classification as determined by Stratus OCT and Cirrus HD-OCT despite an excellent correlation of RNFL thickness measurement. Overall sensitivity and specificity were higher with Cirrus OCT. These findings are particularly relevant when an individual undergoes longitudinal follow-up with different OCTs.

- Assessment of glaucoma risk

- OHTS HRT ancillary study showed positive predictive value of CSLO ONH examination at baseline
- Similar findings with SLP and OCT in different datasets

Zangwill LM, Weinreb RN, Balcer JA, et al. Baseline topographic optic disc measurements are associated with the development of primary open-angle glaucoma: the Confocal Scanning Laser Ophthalmoscopy Ancillary Study to the Ocular Hypertension Treatment Study. Arch Ophthalmol 2005;123:1188–1197.

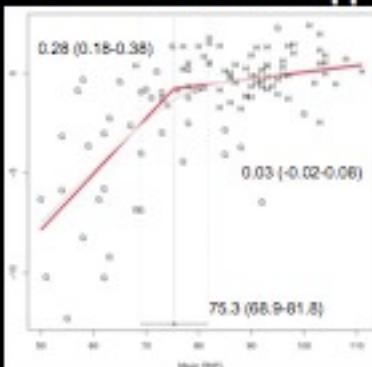
Mohammadi K, Bowd C, Weinreb RN, et al. Retinal nerve fiber layer thickness measurements with scanning laser polarimetry predict glaucomatous visual field loss. Am J Ophthalmol 2004;138:592–601.

Lakkaraju M, Medeiros FA, Weinreb RN, et al. Baseline Optical Coherence Tomography Predicts the Development of Glaucomatous Change in Glaucoma Suspects. Am J Ophthalmol 2006;142:576–582.

## Clinical Application of SD-OCT in Glaucoma

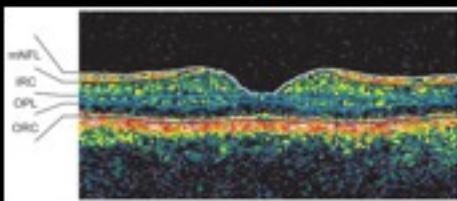
- Structure before function?

- RNFL thickness “tipping point”

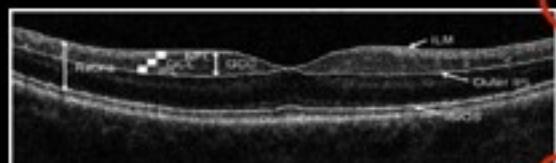


RNFL	Tipping Point (μm)	95% CI (μm)
Mean	75.3	68.9–81.8
Temporal	51.1	46.6–55.6
Superior	83.0	76.3–89.7
Nasal	70.2*	52.7–87.7
Inferior	87.5	73.6–101.4

# The Macula as a Glaucoma Diagnostic Target



Yilmaz H, Sohn DM, Wolfsen G, Schuman JS, Holmes JD, Schuman JS, Meyer Segmentation with Optical Coherence Tomography. Invest Ophthalmol Vis Sci. 2009 Jun; 50(6):1-20. Epub 2009 Mar 1.

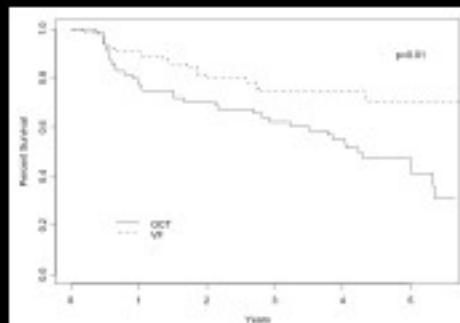


Diagnostic Parameter	PG AROC (SE)	PPG AROC (SE)
<b>RTVue ED-OCT</b>		
GOC-AVG (μm)	0.80 (0.02)	0.78 (0.05)
GOC-FLV (%)	0.82 (0.02)	0.73 (0.06)
GOC-GLV (%)	0.82 (0.02)	0.79 (0.04)
GOC-TAVG (μm)	0.80 (0.02)	0.72 (0.05)
RNF-AVG (μm)	0.85 (0.02)	0.80 (0.05)
<b>Stratus TD-OCT</b>		
RNF-AVG (μm)	0.82 (0.02)	0.80 (0.05)
RNF-AVG (μm)	0.85 (0.02)	0.76 (0.05)

Tan OJ, Chopra V, Lu AT, Schuman JS, Yilmaz H, Wolfsen G, Verma R, Huang D. Detection of macular ganglion cell loss in glaucoma by Fourier-domain optical coherence tomography. *Ophthalmology* 2009 Dec; 116(12):2309-14.e1-3. Epub 2009 Sep 15.

## Optical Coherence Tomography for Detection of Progression

### Optical Coherence Tomography Longitudinal Evaluation of Retinal Nerve Fiber Layer Thickness in Glaucoma



- >64 eyes/37 glaucoma suspects and glaucoma patients
- Median flu 4.7 years, median 5 usable OCTs and 6 usable VFs
- 66% stable, 22% progressed by OCT alone, 9% by VF alone, 3% by both OCT and VF

Wolfsen G, Schuman JS, Price LL et al: Optical Coherence Tomography Longitudinal Evaluation of Retinal Nerve Fiber Layer Thickness in Glaucoma. *Arch Ophthalmol* 2005; 123:464-470

## Detection of Glaucoma Progression with Stratus OCT Retinal Nerve Fiber Layer, Optic Nerve Head, and Macular Thickness Measurements

Felipe A. Medeiros, Linda M. Zengerrill, Encarna M. Alencar, Christopher Board, Pamela A. Saigal, Renzo Sustavaia, Jr., and Robert N. Weinreb

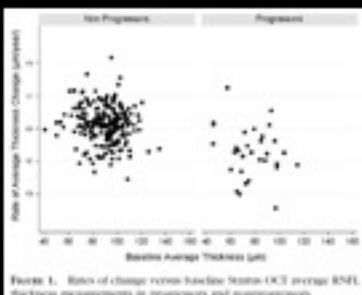


FIGURE 1. Rates of change versus baseline Stratus OCT average RNFL thickness measurements in progressors and non-progressors.

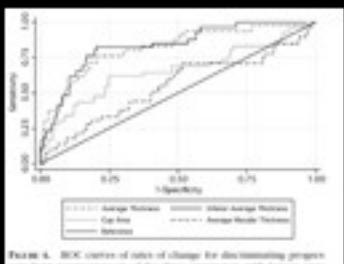


FIGURE 4. ROC curves of rates of change for discriminating progression from nonprogression of the three parameters with largest areas under the ROC curves in each scanning area and the average RNFL thickness.

- 253 eyes, 31 progressors, 4 years median flu
- Progression by GPA versus ONH stereophotograph
- Rate of change -0.72 um/yr versus 0.14 um/yr
- RNFL better than ONH and macula

## Evaluation of Retinal Nerve Fiber Layer Progression in Glaucoma: A Study on Optical Coherence Tomography Guided Progression Analysis

Christopher Kuan-Shun Leung,<sup>1,2</sup> Carol Yim-Tai Cheung,<sup>1</sup> Robert N. Weinreb,<sup>1</sup>  
 Kunlong Qiu,<sup>3,4</sup> Shu Liu,<sup>3</sup> Haitao Li,<sup>3</sup> Guibiao Xu,<sup>3,4</sup> Ning Fan,<sup>3</sup> Chi-Pui Pang,<sup>1</sup>  
 Kwok-Kay Tsui,<sup>4</sup> and Dennis Shan-Chien Lam<sup>1\*</sup>

(Accepted manuscript version; available online March 2010)

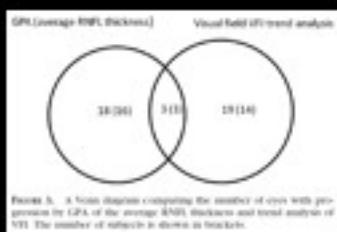
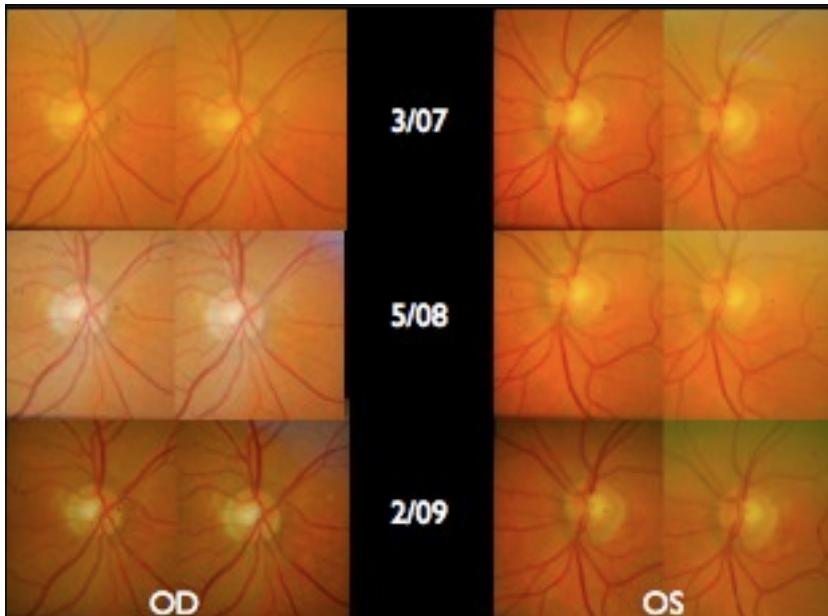


Figure 5. A Venn diagram comparing the number of eyes with progression by GPA of the average RNFL thickness and trend analysis of VF. The number of subjects is shown in brackets.

- 116 eyes of 64 patients, first and last measurements at least 3 years apart
- Progression by OCT GPA versus SAPVR
- Median rate of change -3.3 um/yr versus 3.0%/yr
- Little overlap between VF progressors and OCT progressors

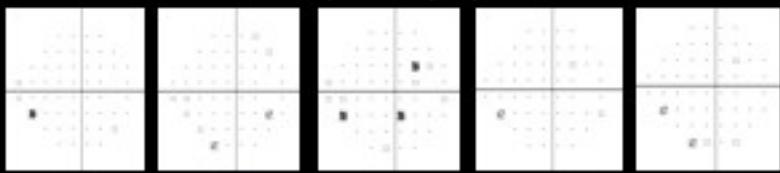
## Case

- 75 year old man
  - H/O round retinal hole
- POAG OU
- Nuclear Sclerotic Cataract OS
- Pseudophakia OD
- VA: 20/25, 20/32
- IOP: 14/18
- CCT: 585/577
- CDR: 0.8/0.8



## Case:Visual Field OD

Pattern Deviation Plots



2001

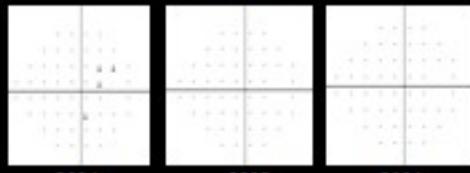
2002

2004

2005

2006

GPA Plots



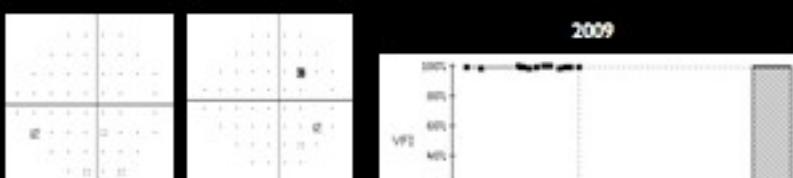
2004

2005

2006

## Case:Visual Field OD

Pattern Deviation Plots



2008

2009

2009

Rate of Progression: +0.0 to +0.1%/year (95% confidence)

Slope not significant

## Case:Visual Field OS

Pattern Deviation Plots



2001

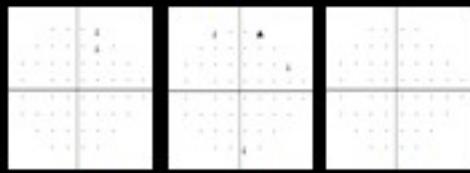
2002

2004

2005

2006

GPA Plots



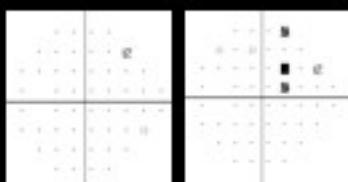
2004

2005

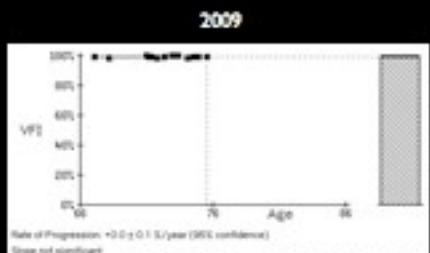
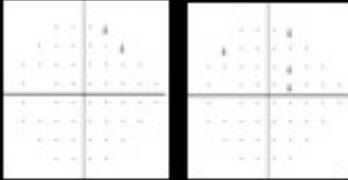
2006

# Case: Visual Field OS

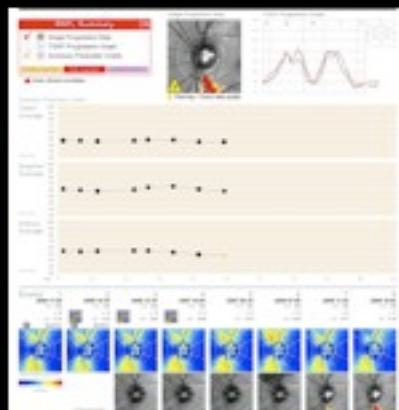
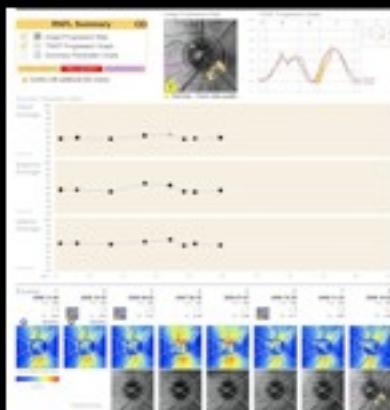
Pattern Deviation Plots



GPA Plots



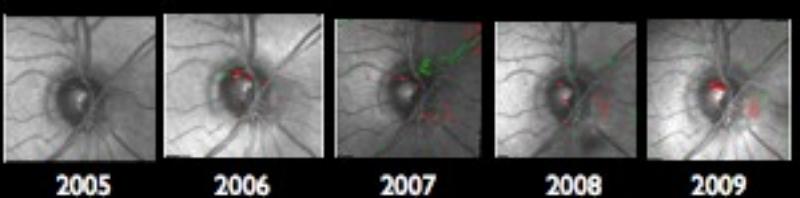
# Case: GDx



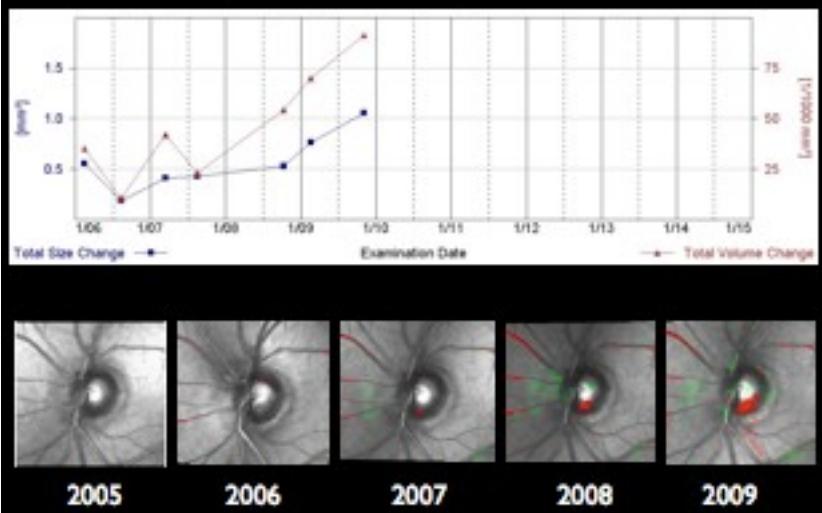
OD

OS

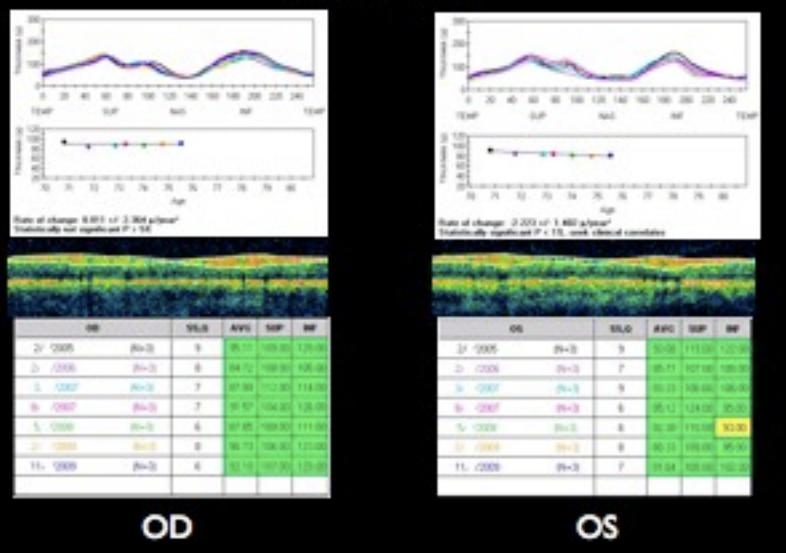
# Case: HRT TCA OD



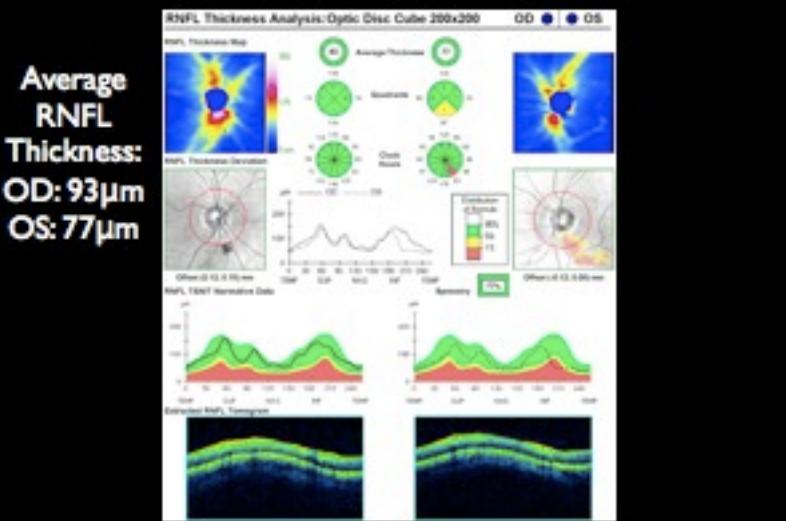
## Case: HRT TCA OS



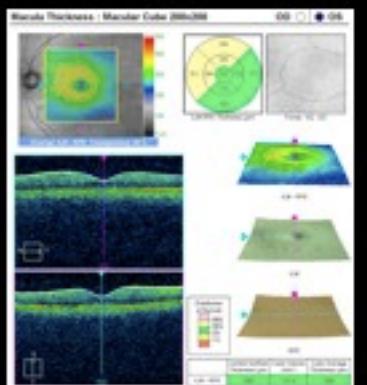
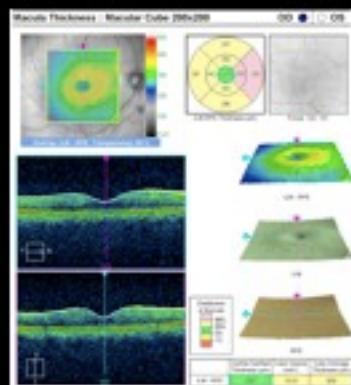
## Case: TD-OCT



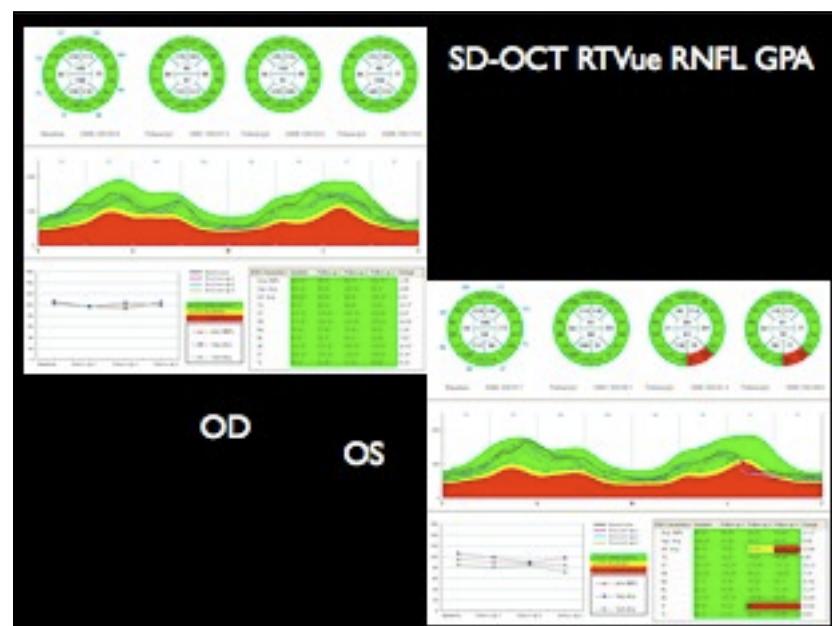
## Case: SD-OCT Cirrus 11/09



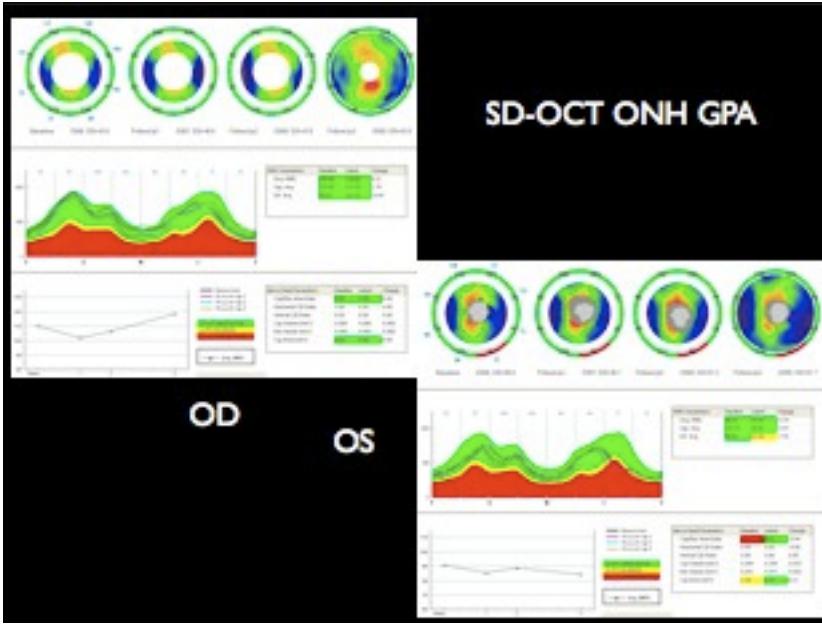
# Case: SD-OCT Cirrus 11/09

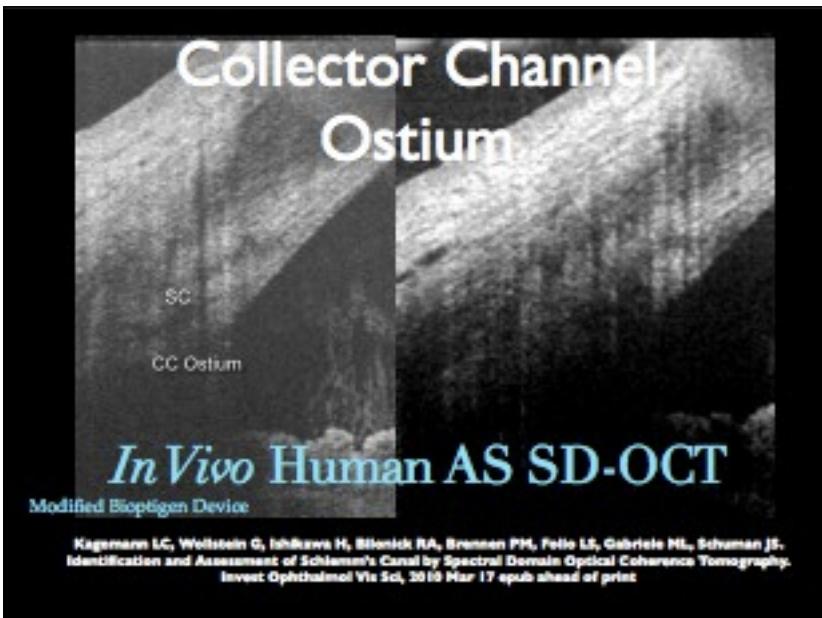
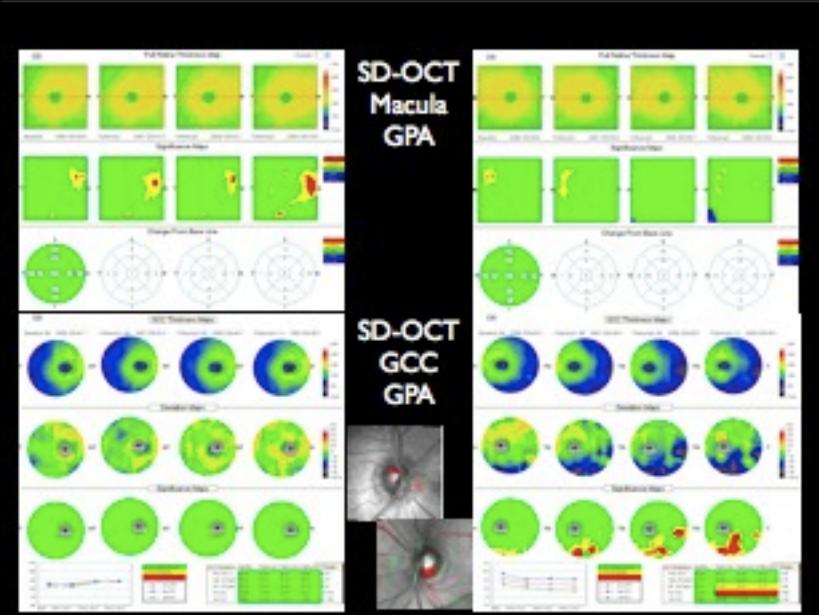


SD-OCT RTVue RNFL GPA



SD-OCT ONH GPA



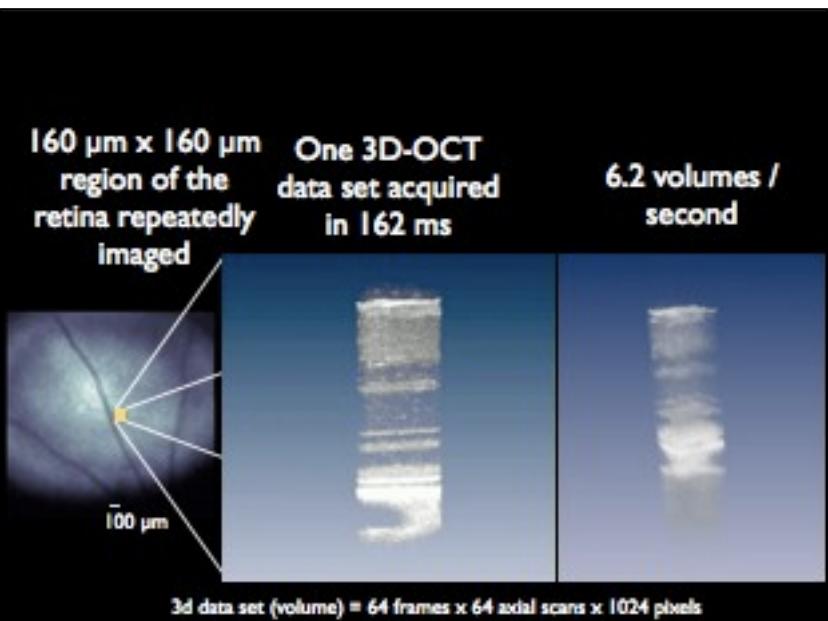




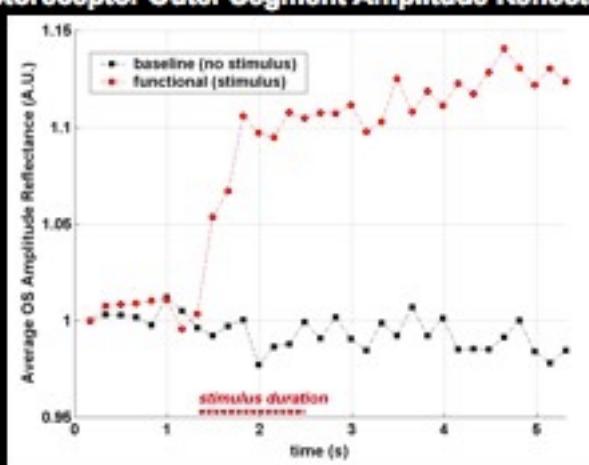
## In Vivo Human AS SD-OCT

Modified BiOptigen Device

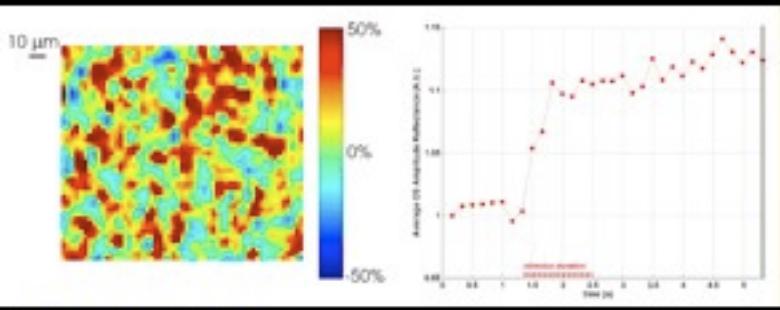
Kagemann LC, Wollstein G, Ishikawa H, Blidenick RA, Brennen PM, Petito LS, Gabriele MS, Schuman JS. Identification and Assessment of Schlemm's Canal by Spectral Domain Optical Coherence Tomography. Invest Ophthalmol Vis Sci, 2010 Mar 17 epub ahead of print.



## Baseline vs. Stimulus Photoreceptor Outer Segment Amplitude Reflectance



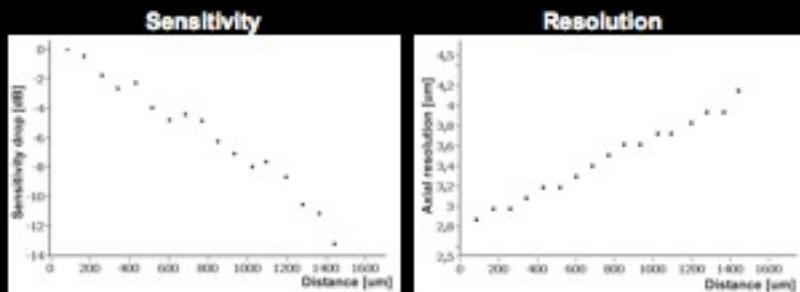
## **En Face View of Functional Response Photoreceptor Outer Segments**



- 160  $\mu\text{m}$  x 160  $\mu\text{m}$  region
- Differential response in color scale (above left)
- Average normalized response shown in scatter plot (above right)

Srinivasan, et al Optics Letters (2006)

## **Limitations of Spectral / Fourier Domain OCT**

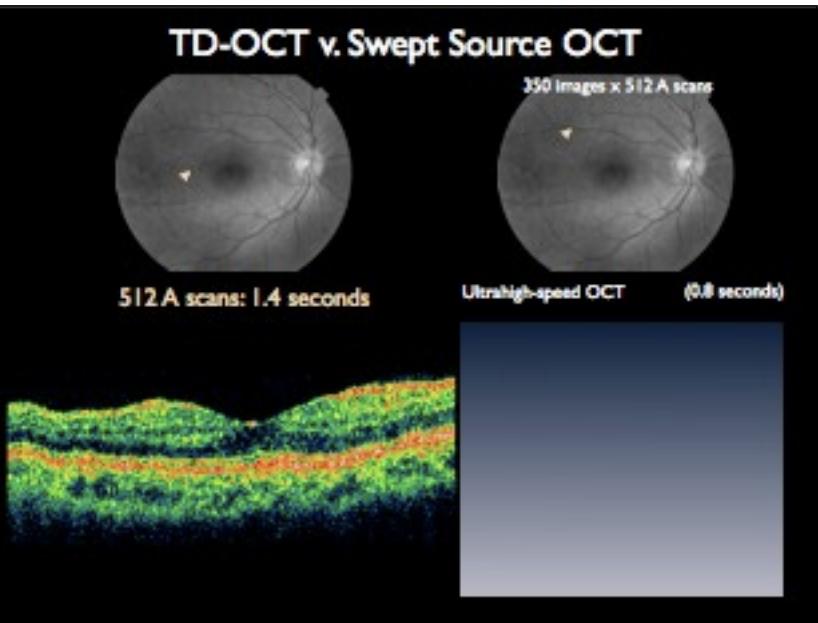


- Sensitivity varies with depth
- Resolution varies with depth
- Speed is limited by CCD camera speeds
- Resolution / depth trade off - limited by number of CCD pixels

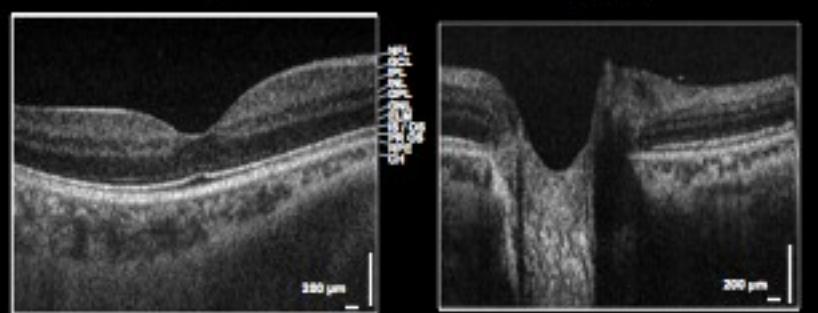
## **High Speed OCT using Frequency Swept Lasers**

- "Swept Source / Fourier domain" detection enables dramatic improvements in speed and sensitivity
- ~500x higher speed than standard OCT
- No spectrometer or CCD required
- Uses high speed single or dual channel A/D
- Can operate at 1 and 1.3  $\mu\text{m}$  wavelengths
- Requires narrow linewidth, high speed, frequency swept lasers

## TD-OCT v. Swept Source OCT



## High Definition Imaging



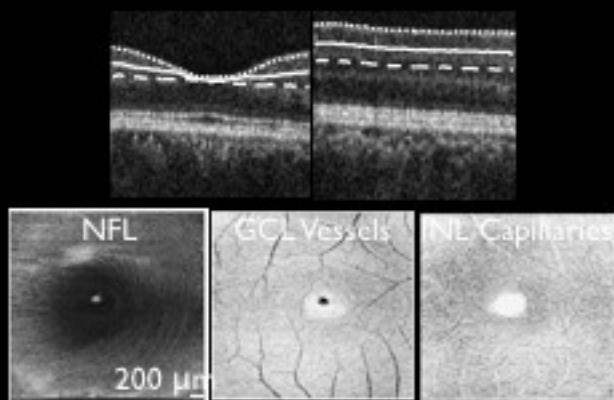
~16,000 axial scans per image

~8 micron resolution in retina

Improved choroidal penetration at 1050 nm

Srinivasan V, Adler D, Chen Y, Gorczyca I, Huber R, Dulker J, Schuman JS, Fujimoto J. Ultrahigh-speed Optical Coherence Tomography for Three-Dimensional and En Face Imaging of the Retina and Optic Nerve Head. *Ophthalmology*. November 2008; Vol.115, No. 11, S103-S110.

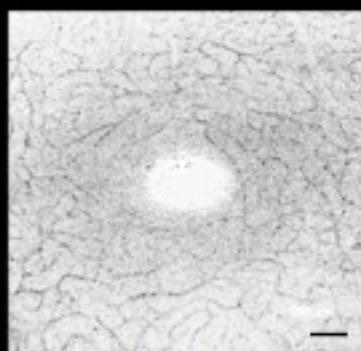
## En Face Imaging of Inner Retina



512 x 850 axial scans, 2 s

Srinivasan V, Adler D, Chen Y, Gorczyca I, Huber R, Dulker J, Schuman JS, Fujimoto J. Ultrahigh-speed Optical Coherence Tomography for Three-Dimensional and En Face Imaging of the Retina and Optic Nerve Head. *Ophthalmology*. November 2008; Vol.115, No. 11, S103-S110.

## Imaging of capillaries near the foveal avascular zone



Confocal micrographs of the foveal avascular zone (FAZ) in a retinal wholemount from a young adult macaque monkey (modified from Provis et al. 2000).

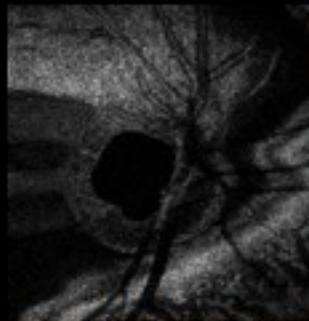
The endothelial cells are

immunocytochemically labeled with antibodies to CD31 and Von Willebrand's factor.

512 x 850 axial scans, 2 s

Srinivasan V, Adler D, Chen Y, Gorczyca I, Huber R, Duke J, Schuman JS, Fujimoto J. Ultrahigh-speed Optical Coherence Tomography for Three-Dimensional and En Face Imaging of the Retina and Optic Nerve Head. IOVS; November 2000;Vol.41, No. 11, 5103-5110.

## En Face Imaging of the Lamina Cribrosa



Scanning Electron Microscope Image of the Lamina Cribrosa. From Jonas et. al, IOVS, 1991

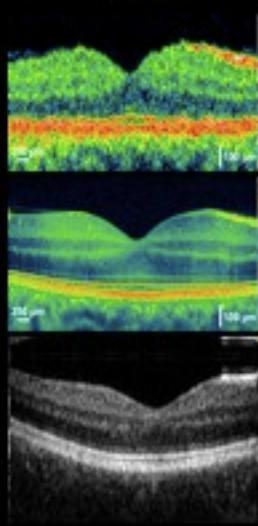
En Face depth sectioning using ultrahigh speed OCT

512 x 450 axial scans, 1 sec

Srinivasan V, Adler D, Chen Y, Gorczyca I, Huber R, Duke J, Schuman JS, Fujimoto J. Ultrahigh-speed Optical Coherence Tomography for Three-Dimensional and En Face Imaging of the Retina and Optic Nerve Head. IOVS; November 2000;Vol.41, No. 11, 5103-5110.

## OCT technologies for retinal imaging

- Time-domain OCT
  - 400 axial scans per second
  - 1 (500 pixel) image per second
  - Zeiss StratusOCT
- Spectral / Fourier domain OCT
  - ~25,000 - 55,000 axial scans per second
  - ~100 - 200 images per second
  - >7 companies marketing instruments
- Swept source / Fourier domain OCT
  - ~250,000 axial scans per second
  - ~500 images per second
  - Resolution lower than spectral OCT
  - Currently in the research stage



## SD-OCT

- Limitations
  - The technology is young, still in evolution.
  - OCT imaging may be difficult in the presence of media opacities such as dense central corneal scarring, severe posterior subcapsular cataract, dense vitreous hemorrhage
  - SD-OCT still requires development of robust alignment and registration algorithms to approach its clinical potential

## OCT in Glaucoma

- Optical Coherence Tomography (OCT) is a useful tool for the assessment of the presence or absence of glaucoma and its progression
  - Structure – function correlates
  - Identify areas of abnormality or change
  - Reduce uncertainty in Glaucoma Suspects
- 3D OCT imaging increases reproducibility, and may enhance sensitivity and specificity
- OCT statistical software for the measurement of glaucoma progression is now commercially available

## The Future of OCT - Where Are We Going?

- Novel diagnostics are at hand for assessment of disease and its progression
- Current commercially available technology may be used in new ways to assess disease and progression

# Collaboration

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Gary Miller, PhD  
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David Tolliver, PhD

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## Copernicus U.

Maciej Wojtkowski, PhD

## Christian Doppler Institute, Vienna

Wolfgang Drexler, PhD

36 Fujimots, 9 Huang and 26 Schuman have IP owned by MIT and licensed to Carl Zeiss  
Wojtkowski, 9 Woldstein and 26 Schuman have IP owned by U. Pittsburgh and licensed to Optigen

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